In Vitro Toxicity and Chemical Characterization of Aerosol Derived from Electronic Cigarette Humectants Using a Newly Developed Exposure System

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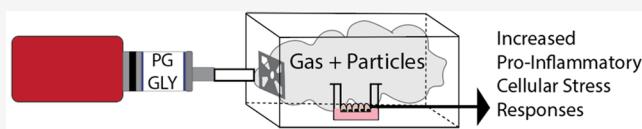
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ABSTRACT: In the United States, the recent surge of electronic cigarette (e-cig) use has raised questions concerning the safety of these devices. This study seeks to assess the pro-inflammatory and cellular stress effects of the vaped humectants propylene glycol (PG) and glycerol (GLY) on airway epithelial cells (16HBE cells and differentiated human bronchial epithelial cells) with a newly developed aerosol exposure system. This system allows for chemical characterization of e-cig generated aerosol particles as well as *in vitro* exposures of 16HBE cells at an air−liquid interface to vaped PG and GLY aerosol. Our data demonstrate that the process of vaping results in the formation of PG- and GLY-derived oligomers in the aerosol particles. Our *in vitro* data demonstrate an increase in pro-inflammatory cytokines IL-6 and IL-8 levels in response to vaped PG and GLY exposures. Vaped GLY also causes an increase in cellular stress signals HMOX1, NQO1, and carbonylated proteins when the e-cig device is operated at high wattages. Additionally, we find that the exposure of vaped PG causes elevated IL-6 expression, while the exposure of vaped GLY increases HMOX1 expression in human bronchial epithelial cells when the device is operated at high wattages. These findings suggest that vaporizing PG and GLY results in the formation of novel compounds and the exposure of vaped PG and GLY are detrimental to airway cells. Since PG and/or GLY is universally contained in all e-cig liquids, we conclude that these components alone can cause harm to the airway epithelium.

1. INTRODUCTION

The rising popularity of electronic cigarettes (e-cigs) has established a billion-dollar industry that is expected to surpass traditional tobacco sales by the year 2047.[1] In the United States, over 10 million adults are current e-cig users, with the majority of users being younger than 35 years old.[2] The increased use of e-cigs is also seen in high school and middle school students in the United States, where it is estimated that over 3 million students have used an e-cig within the last 30 days.[3] While the use of e-cigs has drastically increased, the research to determine the long-term health effects of e-cig use are currently unknown.[4] In short-term (5−14 day) human studies, where smokers were asked to switch to e-cigs, there was a decrease in exposure to carcinogens and improvement in chest tightness.[5] However, in other cross-sectional studies comparing e-cig users to nonsmokers and cigarette smokers, e-cig users have been shown to have respiratory effects that differ from smokers, such as a downregulation of immune genes[6] as well as altered levels of innate defense proteins[7] and altered neutrophil cell function in the airways.[8] There is also a growing field of *in vitro* research on the effects of specific e-cig components, such as flavorings, on the airways.[9−17] Less focus has been on the e-cig humectants, propylene glycol (PG) and glycerol (GLY), which make up the bulk of the e-cig liquid and are common to all nicotine containing e-cig liquids. PG and GLY, when heated in an e-cig, undergo thermal degradation and are known to form aldehydes such as formaldehyde, acetaldehyde, and acrolein.[18] Furthermore, both PG and GLY, when vaporized by an e-cig, form free radicals.[19,20] There are a few *in vitro* studies that examined the effects of vaped PG and GLY,[10,11,21] and the results were varied across studies. Some of these studies showed slight or no adverse effects of PG and GLY exposures on macrophages and airway cells.[11,21] One study using both *in vitro* and *in vivo* models found that vaped PG and GLY resulted in an increase in MUC5AC, which is associated with inflammatory related diseases such as COPD.[7] Recently, a pilot clinical trial had nonsmoking and nonvaping subjects use an electronic cigarette that only contained PG and GLY for a month and found no significant differences in the differential cell counts and pro-inflammatory cytokines between the vaping and nonvaping subjects. However, there was a significant correlation between urinary PG levels measured in vaping subjects and increased cell counts and pro-inflammatory cytokines such as IL-8. These mixed findings likely result from (1) a diversity of e-cig devices available to
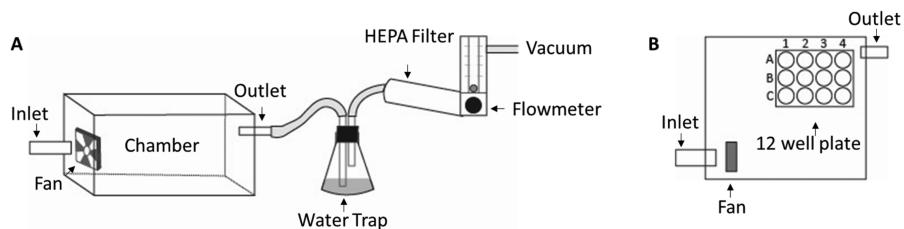
Figure 1. Experimental setup: (A) Exposure system for e-cig generated aerosol and (B) top view of the exposure chamber with placement of the transwell plate used for chemical characterization or *in vitro* exposures.
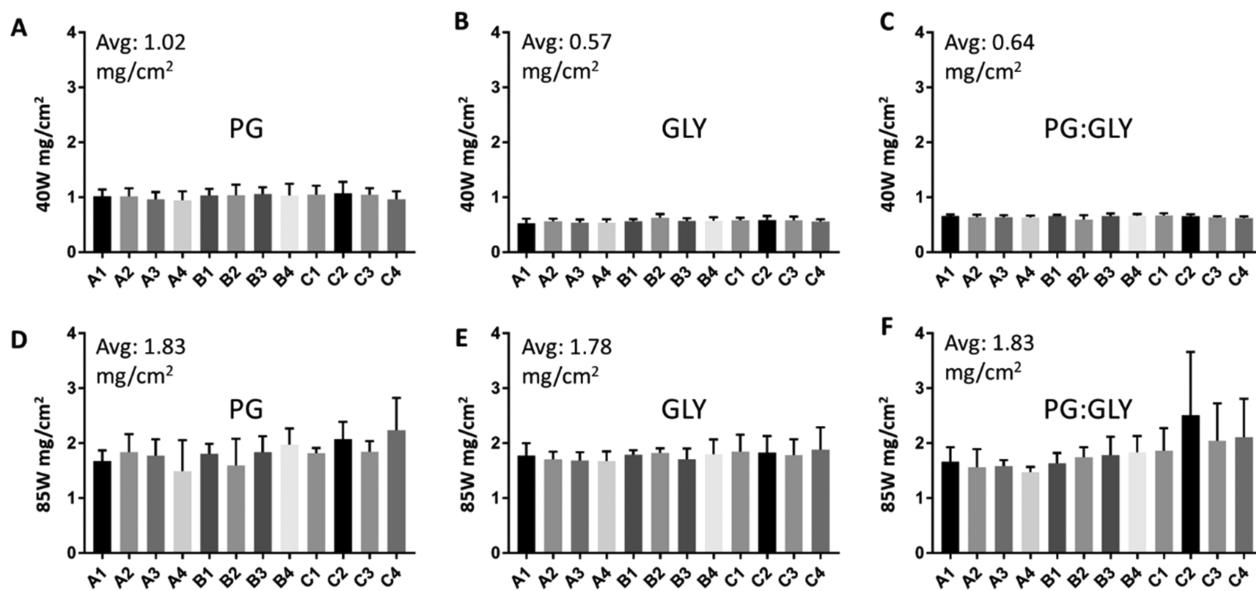

Figure 2. Particle depositions at 40 and 85 W. Mean ± SD. ANOVA followed by post-hoc Tukey's HSD test, $n = 2-3$.

users and researchers, (2) lack of chemical characterization of particulate constituents produced by e-cigs as a function of initial e-liquid composition and operator settings, and (3) a variety of exposure methods used by the scientific community.

There are currently a limited number of commercially available aerosol exposure systems for e-cig research. These systems are generally smoking machines with associated exposure chambers that have been retrofitted to perform e-cig exposures.[22,23] In this study, we designed and optimized an exposure system that can be used to characterize the chemicals in the e-cig generated (vaped) aerosol and expose cells at an air−liquid-interface (ALI) to the whole vaped aerosol. Our system allows for substantial and uniform deposition of e-cig aerosol, chemical characterization of the aerosol mixture or exposure of cells in an *in vitro* setting, and determination of biological effects. Using this optimized exposure system, we conducted a series of *in vitro* exposures to determine aerosol composition and epithelial cell responses induced by aerosols from vaporized pure PG and GLY solutions as well as a mixture thereof. We hypothesized that vaped PG and GLY would induce a pro-inflammatory and cellular stress response from the exposed airway epithelial cells.

2. METHODS

A bespoke aerosol exposure chamber was used to expose either cells to the aerosols of vaped humectants PG and GLY or collect the aerosol on glass coverslips. The e-cig device and exposure system are described below. Chemical characterization conducted in the absence

of cells is described in sections 2.2−2.4, and the *in vitro* cell exposures are described in sections 2.5−2.13.

2.1. E-Cig Device, E-Liquids, and Exposure System. A third generation DNA 200 Lava Box with a SMOK TFV4 mini tank using a sub-ohm TF-S6 sextuple kanthal coil was used for all exposures. The e-cig device was operated at either 40 or 85 W, which are within the manufacturer's suggested range of 30−100 W. Pure PG (Fischer, USP grade), pure GLY (Aldrich, USP grade), and 55:45 v/v PG/GLY mixtures were vaporized using separate tanks. The e-cig tanks were filled with humectant prior to vaping and maintained at ≥two-third tank capacity during exposure to avoid dry puffing conditions.

Figure 1A shows the exposure system. A $17.8 \times 17.6 \times 10.0$ cm^3 Plexiglas chamber was used for e-cig exposures. At the front-left corner of the chamber, an inlet port was constructed into which the e-cig device is inserted and operated to mimic vaping. The inlet was sealed with a rubber stopper when the e-cig was not being operated. A brushless fan (YaKoo DC Model DC12 V) was mounted inside the chamber in front of the inlet to circulate the incoming e-cig aerosol. The fan could be turned on and off from outside the chamber. Outlet tubing was attached to the back-right corner of the chamber, which in turn was connected to a water trap followed by a HEPA capsule filter (Product No. 12144, Gelman Sciences) to collect outgoing e-cig aerosol before reaching the flow meter (Dwyer, Inc.) and the vacuum line.

2.2. Exposure Parameters. Before each exposure, all e-cig tanks were filled completely with their respective humectant. During the exposure, humectant levels within the tank were monitored not to go below two-thirds full to avoid the chance of dry puffing conditions. The e-cig mouthpiece was inserted into the inlet and turned on for 4 s at a flow rate of 2.5 L per minute for a puff volume of 166 mL, followed by a 26 s interpuff period during which the chamber was sealed. Previous studies have recommended that e-cigarette laboratory

experiments use 4 s puffs with a 20−30 s interpuff interval.[24] For experiments described here, each exposure lasted 10 min, with a total of 20 puffs per exposure. E-cigarette topography studies have shown that puff duration can range from 2 to 8 s[24−28] and that puff volumes can range from less than 37 to over 176 mL.[28] While our puffing volume of 166 mL is on the higher end of published topography studies, it is well below the average tidal volume of 500 mL.

2.3. Aerosol Deposition on Glass Coverslips. Uniformity of aerosol deposition and composition of generated aerosols were tested in experiments using glass coverslips (8 mm) placed into a 12 mm transwell cell culture plate (Fischer Scientific 07200161; Figure 1B). E-cig exposures were completed with PG/GLY ratios of 100:0 (PG), 0:100 (GLY), and 55:45 (PG/GLY) using the previously described exposure parameters. The e-cig device was operated at either 40 or 85 W, which are within the manufacturer's suggested range of 30−100 W. Coverslips were weighed using a microbalance (Mettler Toledo) immediately before and after e-cig exposure to determine the quantity and distribution of aerosol deposited on the sampling area (Figure 2). These experiments were repeated three times ($n = 3$). In some experiments, following weighing, three glass coverslips from each exposure were transferred to 20 mL precleaned borosilicate scintillation vials for immediate extraction and subsequent chemical composition analysis within 12 h.

2.4. Chemical Characterization of Samples by UPLC/ESI(+)-HR-QTOFMS. Three glass coverslips from each aerosol deposition experiment were immersed in 1 mL of 50:50 (v/v) methanol/water mixture and were extracted for 10 min by ultrasonication. Samples were analyzed by ultraperformance liquid chromatography coupled with electrospray ionization high-resolution quadrupole time-of-flight mass spectrometry operated in positive ion mode (UPLC/ESI(+)-HR-QTOFMS).

UPLC separations were achieved using an Agilent 6500 series UPLC system with a C_{18} column (Waters ACQUITY UPLC HSS T3, 2.1 mm × 100 mm, 1.8 μm particle size) at 45 °C. Mobile phases consisted of A (water with 0.1% ammonium acetate) and B (methanol with 0.1% ammonium acetate). The volume fraction of mobile phase A was ramped at constant flow (0.3 mL min^{-1}) as follows: 100% held for 2 min; ramp 100−10% for 8 min; 10% held for 1 min; ramp 10−100% for 4 min (total 15 min).

ESI(+)-HR-QTOFMS using an Agilent 6520 Series Accurate Mass Q-TOFMS was used to detect PG, GLY, and other compounds. Masses were scanned from 60 to 1000 Da. The TOF mass was continuously corrected by injecting a reference mixture containing purine, leucine enkephaline, and hexakis phosphazine acetate. Sodium chloride was included in this reference mixture such that ionization of target analyte molecules could be achieved by the formation of sodium adducts.

Standards of pure PG and GLY were prepared in 50:50 (v/v) water/methanol mixtures at concentrations of 0.1, 0.25, 1.0, 2.5, 10, and 25 μg mL^{-1}. The calibration was linear through 10 μg mL^{-1}, with coefficients of correlation of $R^2 = 0.9983$ for GLY and $R^2 = 0.9991$ for PG.

2.5. Cell Culture. We used 16HBE14o (16HBE), a gift from Dr. D.C. Gruenert (University of California at San Francisco), an SV-40 transformed bronchial epithelial cell line. 16HBE cells were plated on fibronectin and collagen coated 12 mm transwell plates (Fischer Scientific 07200161) and grown submerged in complete media (MEM with 10% FBS, 1% penicillin−streptomycin, and 1% L-glutamine) for 3 days until reaching 100% confluency. Two days prior to exposures, apical media was removed and the cells were then placed at ALI with complete media in the basolateral compartment for 24 h, followed by replacing the media with less serum containing media (MEM, 2% FBS, 1% penicillin−streptomycin, and 1% L-glutamine) for another 24 h.

Human bronchial epithelial cells (hBECS) were obtained from healthy donors in collaboration with the Environmental Protection Agency (EPA) using a protocol approved by the University of North Carolina at Chapel Hill Institutional Review Board (Chapel Hill, NC), as described previously.[29] The cells were then expanded to passage 2 in in PneumaCult-Ex Plus Medium (Stemcell 05040),

supplemented with hydrocortisone (0.48 μg/mL), penicillin (100U/ml), streptomycin (100ug/mL), and amphotericin B (0.25ug/mL), and then plated on 0.4 μm Transwell plates and cultured in the same media until confluency. Once the cells reached confluency on the transwells the cells were taken ALI with PneumaCult ALI Medium (Stemcell 05001) to promote differentiation. Complete differentiation was achieved 24−28 days post-ALI, and cells were then exposed to the vaped humectants.

2.6. *In Vitro* Exposures. 16HBE cells at ALI were exposed to the aerosol of vaped PG, GLY, and a PG/GLY mixture at a 55:45 v/v ratio with a 4 s puff at a flow rate of 2.5 L per minute, followed by a 26 s interpuff period during which the chamber was sealed. Each exposure lasted 10 min, with a total of 20 puffs per exposure. At 1 h post-exposure, whole cell lysate was collected in RIPA buffer with protease inhibitors (Sigma-Alrdrich P8340). At 2 h post-exposure, cell lysates were collected in Ambion lysis buffer with 1% BME following the protocol from the Pure Link RNA mini kit (Life Technologies 12183025). At 24 h post-exposure, basolateral supernatants (baso sup) and whole cell lysates were collected. These experiments were repeated three times ($n = 3$) for each time point.

Fully differentiated hBECs from a minimum of 3 different donors ($n = 3$) were exposed to the aerosol of vaped PG, GLY, and a PG/GLY mixture at a 55:45 v/v ratio with a 4 s puff at a flow rate of 2.5 L per minute followed by a 30 s interpuff period. Each exposure lasted 10 min with a total of 17 puffs per exposure. At 2 h post-exposure, cell lysates were collected in Ambion lysis buffer with 1% BME following the protocol from the Pure Link RNA mini kit (Life Technologies 12183025).

2.7. Particle Depleted Aerosol *In Vitro* Exposure. In order to filter out the particles from the aerosol of vaped PG, GLY, and PG/GLY, a HEPA filter (GE Healthcare 6702-9500) was placed in line between the inlet of the exposure chamber and the e-cig device mouthpiece. A flow rate calibrator (Gilibrator) was used to ensure that the flow rate through the system was not significantly reduced with the filter in line with the exposure system. Aerosol size distributions were continuously measured using a differential mobility analyzer (DMA, BMI model 2002) coupled to a mixing condensation particle counter (MCPC, BMI model 1710) after each exposure to ensure that the filter did not saturate or allow particles into the chamber. 16HBE cells at ALI were exposed to the gas phase of vaped PG, GLY, and a PG/GLY mixture at a v/v ratio with the previously described exposure parameters. Cell lysates and basolateral supernatants were collected at 2 and 24 h, respectively, and analyzed as described above. These experiments were repeated three times ($n = 3$) for each time point.

2.8. *In Vitro* Exposure of Nonaerosolized PG and GLY Liquid. From the deposition experiments, the mass of particles in each transwell was determined (Figure 2). 16HBE cells on transwells were exposed submerged to the equal mass of particles, diluted in media for 2 h, that had deposited in the 85 W exposures of PG, GLY, and a PG/GLY. Cell lysates and basolateral supernatant were collected at 2 and 24 h, respectively, and analyzed as described above. These experiments were repeated three times ($n = 3$) for each time point.

2.9. Real Time qPCR. Total RNA was isolated from 16HBE cells 2 h post-exposure with the Pure Link RNA Mini Kit (Life Technologies 12183025). RNA was reverse transcribed into cDNA by incubating 400 ng of RNA in a 25 μl buffer containing, 0.05 mM Random Primers (Roche 11034731001), 0.5 mM dNTPs (Promega U151B), RNase inhibitor (Promega N215B), M-MLC-RT (Invitrogen 28025-01), 50 mM KCl, and 2 mM MgCl$_2$, pH 9.3. Following a 50 min incubation at 37 °C, the mixture was heated to 70 °C for 15 min to inactivate reverse transcriptase. The following primers and probers for *HMOX-1* and *NQO1* were commercially available (Applied Biosystems) and IL-6 and IL-8 were prepared in-house: human IL-6 5′-FAMCCAGCATCAGTCCCAAGAAGGCAACTT-AMRA-3′ (probe), 5′-TATGAAGTTCCTCTCTGCAAGAGA-3′ (sense), and 5′-TAGGGAAGGCCGTGGTT-3′ (antisense); 5′-FAMCCTTGGCAAAACTGCACCTTCACTAMRA-3′ (probe), 5′-TTGGCAGCCTTCCTGATTTC-3′ (sense), and 5′-TATGCACTG-
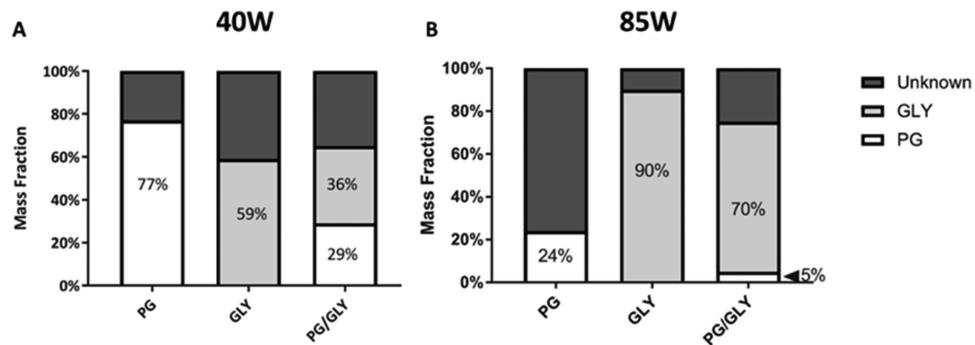
Figure 3. Quantification of PG and GLY as a percentage of collected aerosol mass: pure PG, pure GLY, and 55:45 (v/v) PG/GLY mixture.

ACATCTAAGTTCTTTAGCA-3′ (antisense). Differences in gene expression were determined with the ΔΔCt method and ACTB was used as the normalizing control.

2.10. Cytokine Analysis. Cytokine concentrations were measured in the collected basolateral supernatant from 16HBE 24 h post-exposure. IL-6 and IL-8 cytokine concentrations were determined by enzyme-linked immunosorbent assay (ELISA) according to the manufacturer's instruction (BD Biosciences 555220 and 555244).

2.11. Immunoblot. Whole cell lysate was collected from 16HBE cells at 1 and 24 h post-exposure. The samples collected 1 h post-exposure were used to measure carbonylated proteins using an OxyBlot protein oxidation detection kit (Sigma-Aldrich S7150). To describe the method in brief, we detected protein carbonyl groups by derivatizing them with 2,4-dinitrophenylhydrazine (DNPH). We then separated these derivatized protein samples with a 4−20% Mini-PROTEAN TGX Precast Gel (Bio Rad 4561094) and transferred them to a nitrocellulose membrane. The derivatized proteins were then detected by antibodies specific to the DNP moiety. Densitometry was used to measure the density of all the bands detected for each sample. The data are presented as a fold change over the optical density of all the derivatized protein in the blot. These experiments were repeated three times ($n = 3$).

Whole cell lysate samples collected 24 h post-exposure were separated by 4−20% Mini-PROTEAN TGX Precast Gel (Bio Rad 4561096) and transferred to nitrocellulose membrane. HO-1 was detected using a monoclonal antibody (Abcam ab13248)). β-actin (ACTB) was detected using a monoclonal antibody (Santa Cruz and sc-47778) to serve as a loading control. The primary antibodies were then detected with a horseradish peroxidase-conjugated secondary antibody and were detected by chemiluminescence. The HO-1 protein data are presented as the optical density of HO-1 normalized to the optical density of ACTB of the respective sample. These experiments were repeated three time ($n = 3$)

2.12. Cytotoxicity. 16HBE cell viability was measured 24 h post-exposure by measuring lactate dehydrogenate (LDH) release into the basolateral supernatant following the manufacturer's instructions (Thermo Fisher Scientific, Waltham, MA, USA). We measured 100% cell death (maximal LDH release caused by lysis with 1.0% Triton X-100 in cell culture medium) and baseline LDH release (incubator control cells) to calculate the viability as following:

$$\text{Corrected viability} = 100 - [[\text{Abs}(X) - \text{Abs}(Y)]/[\text{Abs}(MAX) - \text{Abs}(Y)] \times 100]$$

where Abs(X) is the absorbance of the sample, Abs(Y) is the absorbance of media from the untreated control cells, and Abs(MAX) is the absorbance of media collected from cells exposed to 1.0% Triton X-100. These experiments were repeated three times ($n = 3$).

2.13. Statistical Analysis. Data are presented as mean ± standard deviation (SD). For the deposition data, the exposures were repeated three separate times and were analyzed using one-way ANOVAs with a Tukey post-hoc test. For the in vitro 16HBE data, the exposures were repeated three separate times ($n = 3$) and were analyzed by a repeated measures one-way ANOVA followed by a post-hoc

uncorrected Fisher's LSD test. For the hBEC data, the exposures were done with a minimum of three different biological replicates ($n = 3−5$) and were analyzed with a one-sample t test with a hypothetical value of 1. Significance was determined by *$p \leq 0.05$, **$p \leq 0.01$, ***$p \leq 0.001$ as compared to air control.

3. RESULTS

3.1. Validation of E-Cig Exposure System. The initial goal was to develop an e-cig exposure system that is compatible with chemical characterization and in vitro exposures of relevant cell culture models. To validate whether our exposure system could deliver an even exposure within the cell culture plate, we measured the deposition of the aerosols from vaped PG, GLY, and a mixture of PG/GLY using two different wattage settings, 40 and 85 W. Figure 2 shows that there was homogeneous deposition across the different wells (A1−A4, B1−B4, C1−C4) of the plate within each experimental condition (Figure 2). For the 40 W experiments, there was uniform deposition within each respective experiment (i.e., pure PG, pure GLY, and a 55:45 (v/v) mixture of PG:/GLY) but the average mass deposited was different between the vaped humectants. The average masses deposited for the 40 W experiments for pure PG, pure GLY, and 55:45 (v/v) mixture of PG/GLY are as follows: 1.02 ± 0.136, 0.567 ± 0.0549, and 0.642 ± 0.0395 mg/cm², respectively (Figure 2 A, B, and C). Interestingly, the average masses deposited for the 85 W experiments were quite similar to each other and showed no significant differences. The average masses deposited for each exposure at 85 W for pure PG, pure GLY, and 55:45 (v/v) mixture of PG/GLY were 1.83 ± 0.355, 1.78 ± 0.208, and 1.83 ± 0.500 mg/cm², respectively (Figure 2 D, E, and F).

3.2. Chemical Characterization of Aerosol Particles from the Vaped Humectants: PG, GLY, and PG/GLY. Following the validation of the exposure system, we chemically characterized the particle phase of the aerosol from the vaped humectants. PG and GLY aerosols were quantified as the percentage of collected aerosol mass by UPLC/ESI-HR-QTOFMS with authentic standards. In the 40 W experiments, 77% of the mass fraction collected from e-cig generated aerosol of PG was PG, in the GLY experiments, 59% of the mass fraction collected was GLY, and in the PG/GLY experiment, 29 and 36% of the mass fraction were PG and GLY, respectively (Figure 3A). In the experiments using 85 W, 24% of the mass fraction collected from PG-derived aerosol was PG, 90% of the mass fraction collected from GLY-derived aerosols was GLY, and in the PG/GLY-derived aerosol, 5% of the mass fraction collected was PG and 70% was GLY (Figure 3B). These data leave a significant portion of the mass collected as uncharacterized compounds. Nontargeted mass
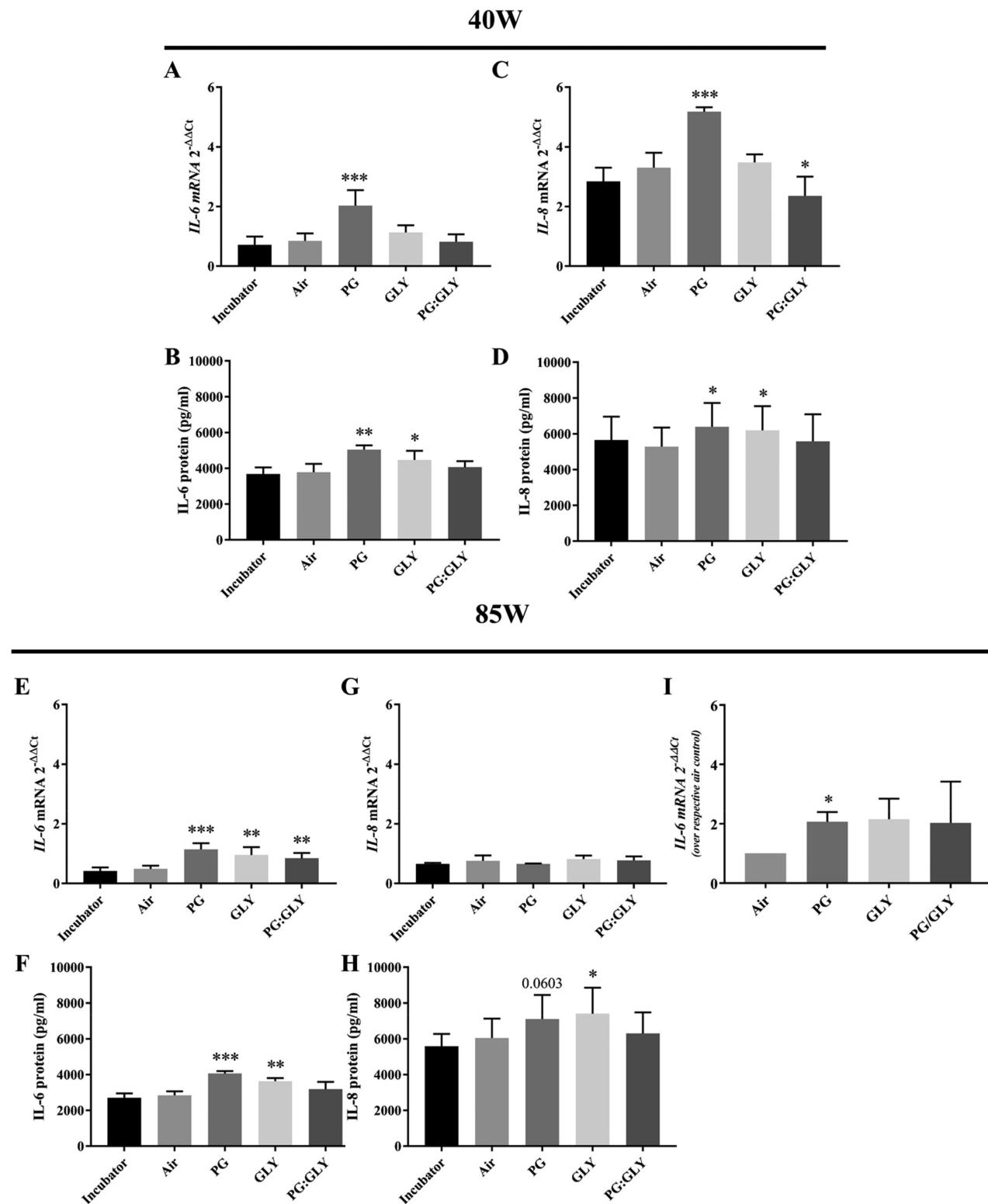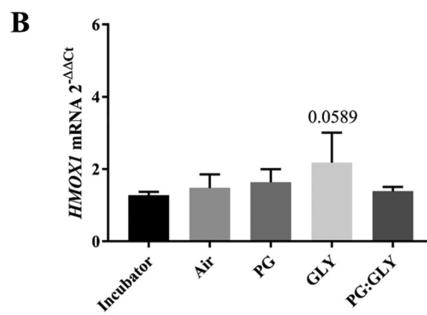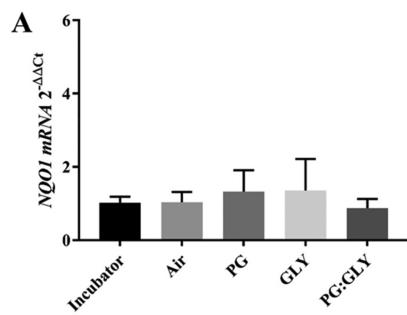
Figure 4. Pro-inflammatory expression at different wattages. (A, C, E, and G) Gene expression of pro-inflammatory cytokines 2 h post-exposure in 16HBE cells. (B, D, F, and H) Protein of pro-inflammatory cytokines 24 h post-exposure in the basolateral supernatant in 16HBE cells. (I) Gene expression of IL-6 2 h post-exposure in hBECs. Three different donors of hBECs were used, $n = 3$. Mean ± SD. $*p \leq 0.05$, $**p \leq 0.01$, and $***p \leq 0.001$ as compared to air control. (A–H) Each experiment was repeated three times, $n = 3$ in 16HBE cells.

spectral analyses conducted with our UPLC/ESI(+)-HR-QTOFMS technique revealed that some of this uncharacterized (unknown) mass is derived from oligomers of PG and GLY. For example, PG-derived aerosols contained dimers with $C_6H_{12}O_2$ and $C_6H_{14}O_3$ molecular formulas and trimers with

$C_9H_{18}O_3$ and $C_9H_{20}O_4$ molecular formulas. GLY-derived aerosols included a dimer with a $C_6H_{12}O_4$ molecular formula and a trimer with a $C_9H_{16}O_5$ molecular formula. Due to the lack of available authentic standards, we cannot conclusively identify their chemical structures, their formation mechanisms,
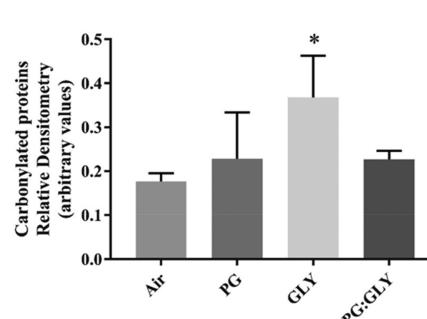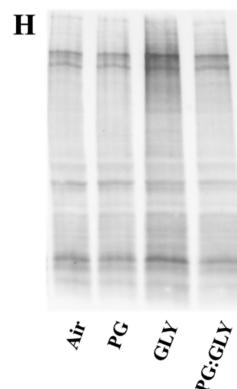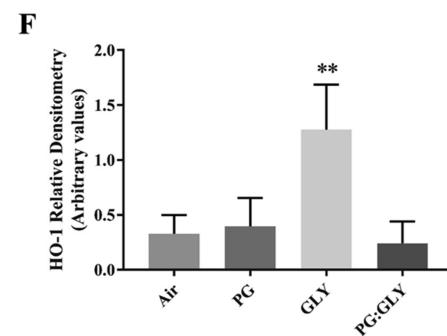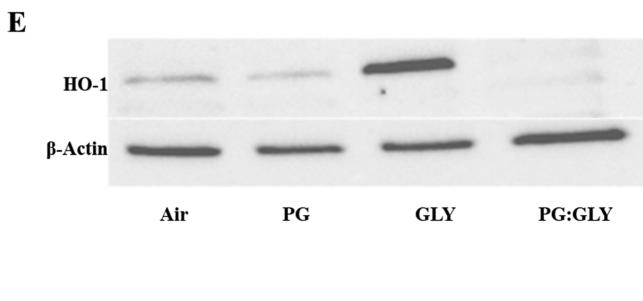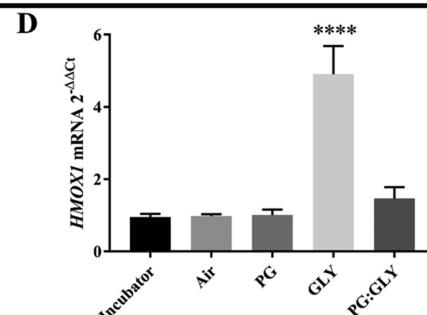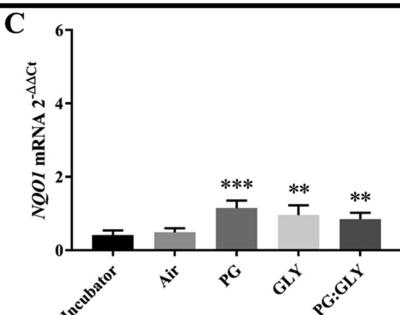
Figure 5. Cellular stress responses at different wattages. (A−D) Gene expression of cellular stress related genes 2 h post-exposure in 16HBE cells. (G) Gene expression of HMOX1 2 h post-exposure in hBECs. Five different biological replicates of hBECs were used, $n = 5$. Mean ± SD. $*p \leq 0.05$, $**p \leq 0.01$, and $***p \leq 0.001$ as compared to air control. (E and H) Representative immunoblot of HO-1 and carbonylated proteins in 16HBE cells. (F and I) Relative densitometry of HO-1 and carbonylated proteins in 16HBE cells. A−F, H, and I) Each experiment was repeated three times, $n = 3$, in 16HBE cells.

or quantitate their contributions to the mass of e-cig aerosol collected during each experiment. However, it is possible that

some of the unknown mass is derived from water that was taken up by PG and GLY during aerosolization and exposure,
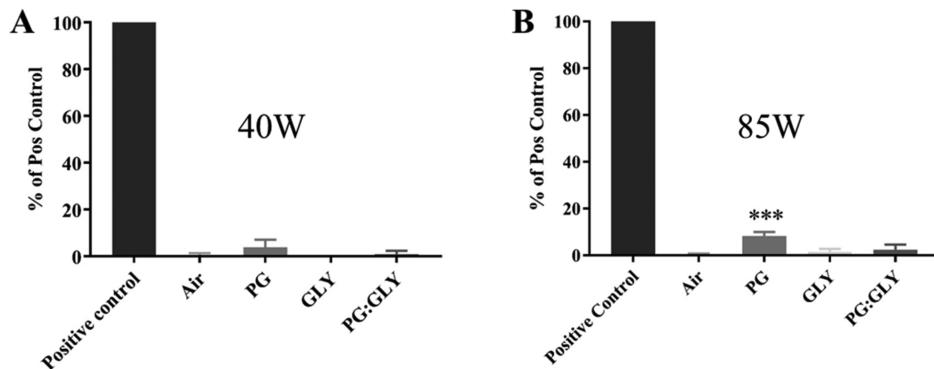
Figure 6. Cytotoxicity of vaped humectant aerosol. (A and B) Cytotoxicity was determined by measuring LDH in 16HBE cells. Mean ± SD. Each experiment was repeated three times, $n = 3$. ***$p \leq 0.05$ as compared to air control.
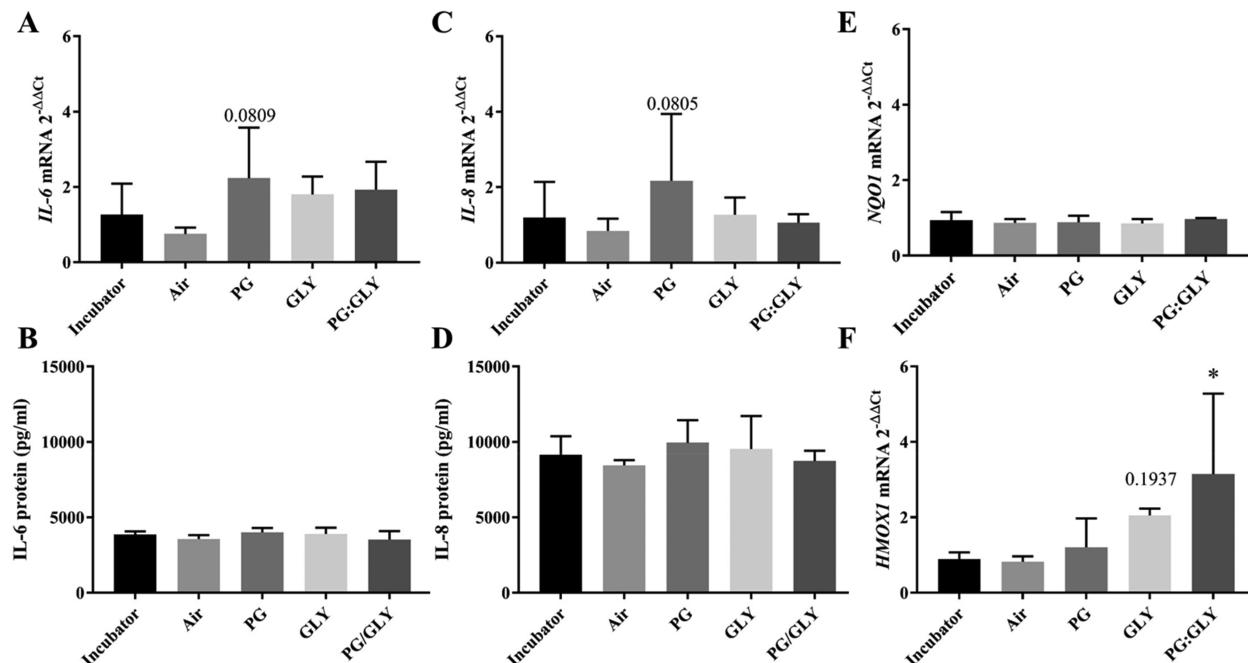

Figure 7. Particle free exposures at 85 W in 16HBE cells. (A, C, E, and F) Gene expression of pro-inflammatory and cellular stress related genes 2 h post-exposure. (B and D) Protein of pro-inflammatory cytokines at 24 h post-exposure in the basolateral supernatant. Mean ± SD. Each experiment was repeated three times, $n = 3$. *$p \leq 0.05$ as compared to air control.

since PG and GLY are hygroscopic compounds[30,31] and likely take up water contained in the air.

3.3. Pro-Inflammatory and Cellular Stress Responses to the Aerosols of Vaped Humectants in Human Airway Epithelial Cells. We used the *in vitro* exposure system to expose a human airway epithelial cell line (16HBEs) at an ALI to the aerosol from vaped pure PG, pure GLY, and a 55:45 (v/v) PG/GLY mixture at 40 and 85 W. Cells were exposed for 10 min and subsequently analyzed for pro-inflammatory cytokine (IL-6 and IL-8) expression. The aerosol of vaped PG at 40 W significantly increased the gene expression and protein levels of IL-6 and IL-8 (Figure 4A–D). Vaped GLY at 40 W did not increase the gene expression of IL-6 or IL-8 2 h post-exposure (Figure 4A,C), but there was an increase in the protein levels of IL-6 and IL-8 at 24 h post-exposure (Figure 4B,D). At 85 W, the aerosols of vaped pure PG, pure GLY, and a 55:45 (v/v) PG/GLY mixture all increased IL-6 expression (Figure 4E) but only vaped PG and GLY increased IL-6 protein levels (Figure 4F). No changes in IL-8 gene expression were measured in any of the 85 W exposures (Figure 4G), but

vaped PG and GLY increased IL-8 protein levels (Figure 4H). We also exposed differentiated human bronchial epithelial cells (hBECs) to the vaped humectants at 85 W. In hBECs exposed to vaped PG, there was an increase in IL-6 expression (Figure 4I) similar to what was seen in the 16HBE cells exposed to vaped PG at 85 W (Figure 4E).

In addition to measuring pro-inflammatory cytokines, we also measured cellular stress responses such as downstream targets of the KEAP1/Nrf2 signaling pathway, HMOX1 and NQO1,[32] which can be upregulated in response to exposures that cause cellular stress such as acrolein,[33] nitric dioxide, and ozone.[34] The 40 W aerosol exposures of vaped pure PG, pure GLY, and a 55:45 (v/v) PG/GLY mixture did not cause any significant changes in NQO1 or HMOX1 gene expression, though the vaped GLY exposure did cause a slight increase in HMOX1 expression (Figure 5A,B) in 16HBE cells. At 85 W, the aerosol of vaped pure PG, pure GLY and a 55:45 (v/v) PG/GLY mixture increased NQO1 gene expression (Figure 5C) and vaped GLY significantly increased HMOX1 expression (Figure 5D) and its corresponding protein, HO-1
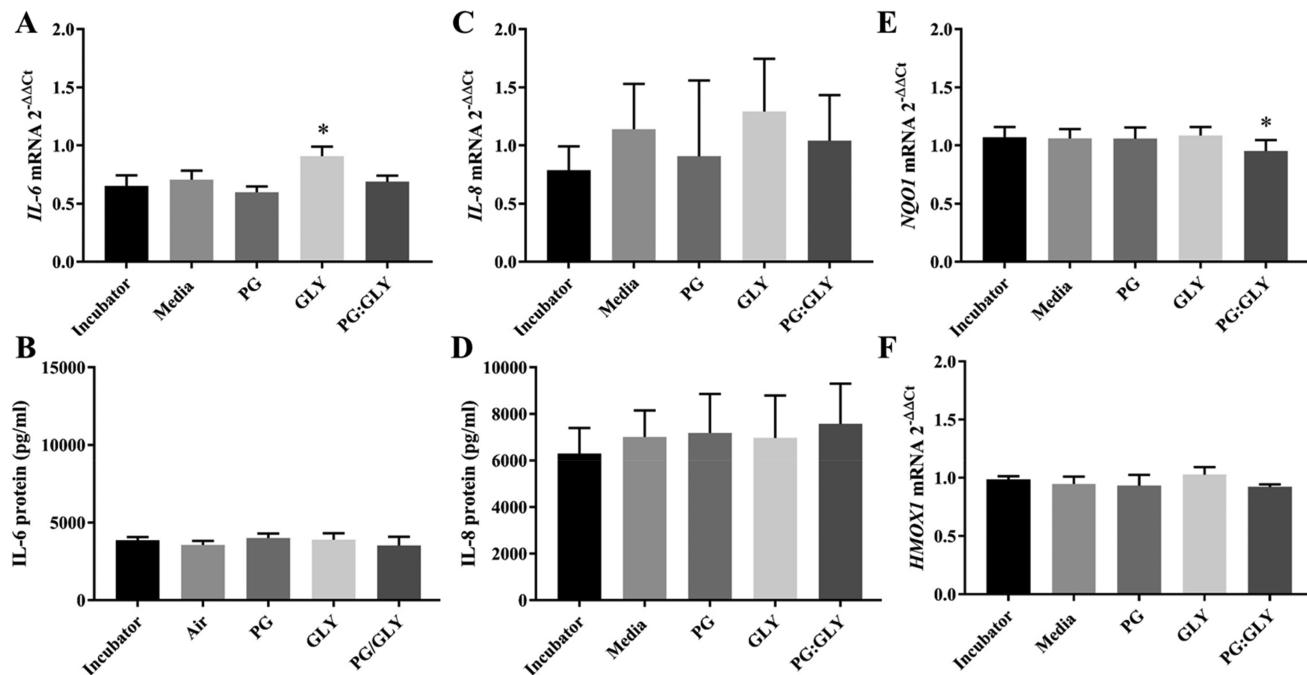
Figure 8. PG and GLY liquid only exposures in 16HBE cells. (A, C, E, and F) Gene expression of pro-inflammatory and cellular stress related genes 2 h post-exposure. (B and D) Protein of pro-inflammatory cytokines 24 h post-exposure. Mean ± SD. Each experiment was repeated three times, n = 3. *$p \leq 0.05$ as compared to air control.

(Figure 5E,F) in 16HBE cells. Similarly, hBECs exposed to the vaped GLY at 85 W also demonstrated an increase in HMOX1 expression (Figure 5G). We went on to measure carbonylated proteins as a marker for oxidative stress for the 85 W exposures (Figure 5H,I) in 16HBE cells. Vaped GLY increased significantly carbonylated proteins as compared to the air control (Figure 5I), suggesting increased oxidative stress.

We determined cytotoxicity induced by the e-cig exposure by measuring the LDH release into the basolateral supernatant of exposed 16HBE cells 24 h post-exposure (Figure 6). Only a modest yet significant increase in LDH release was seen in the vaped PG at 85 W. This exposure caused an 8.2% increase in cytotoxicity as compared to the positive control (Figure 6B).

3.4. Effects of Gas-Phase Components of Vaped Humectants on Airway Epithelial Cells. To remove the particles from the aerosol of vaped humectants at 85 W and to determine whether and to what extent gas-phase components induced the observed effects, a HEPA filter was placed in-line between the inlet of the exposure chamber and the mouth piece of the e-cig device. Cells were exposed to particle-depleted aerosol and assessed for expression of pro-inflammatory cytokines and cellular stress related genes at 2 h post-exposure. IL-6 and IL-8 protein levels were measured at 24 h post-exposure. Similar to the whole aerosol (Figure 4), removing the particles from the PG aerosols still increased, albeit not statistically significant, IL-6 and IL-8 gene expression (Figure 7A,C). However, removing the particles, reduced the effects of GLY aerosol on HMOX1 and NQO1 gene expression (Figure 7E,F as compared to Figure 5C,D).

3.5. Exposure of Nonaerosolized PG and GLY on Airway Epithelial Cells. In order to determine to what extent unaltered PG and GLY in the aerosol affect the end points measured in this study, we exposed cells at ALI to the equal mass of PG, GLY, or PG/GLY deposited in the 85 W exposures (Figure 2 D−F). No changes in IL-8 or HMOX1

gene expression and only moderate changes in IL-6 gene expression were detected (Figure 8A, C, E, and F). However, no changes in IL-6 or IL-8 protein levels were detected (Figure 8B,D). Similarly, no change in HMOX-1 and only a slight decrease was seen in NQO1 expression.

4. DISCUSSION

We have developed and characterized an e-cig aerosol exposure system that is versatile to allow for several different exposures, chemical characterization of aerosol particles, as well as in vitro assessment of biological effects. Our data demonstrate that this exposure system has a uniform deposition across tissue culture plates used in an in vitro experiment (Figure 2). We also show that the entire aerosol mixture from vaped humectants, PG and GLY, cause differential responses (Figures 4 and 5) and that gas-phase components of the aerosol contribute to the pro-inflammatory effects and cellular stress responses within exposed cells (Figure 7). Furthermore, chemical transformations occurring during the vaporization process are important for biological responses, since direct exposures of equivalent nonvaped pure PG and GLY failed to induce the same biological responses as seen with vaporized PG and GLY (Figures 4, 5, and 8).

Our system also allows for a greater deposition than other commercially available exposure systems that have been used for e-cig aerosol exposures.[22,23] There are several potential reasons for these differences; our system has no tubing between the mouthpiece of the e-cig device and the inlet of the exposure chamber, while other systems such as the RM20S and VC10 have 2.9 m and 0.9 m of tubing, respectively.[22] Tubing could potentially cause wall-loss of the aerosol mixture. In addition, exposure systems like the VC1, VC10, and VC6/4, generally dilute the aerosol that is generated by the e-cigarette prior to exposure of airway epithelial cells.[7,35−37] In contrast, the exposure system described in this study does not dilute the

aerosol and has no tubing, thus providing a direct exposure of the aerosol mixture generated by the e-cigarette device.

We demonstrate more particle deposition in the 85 W exposures (Figure 2 D−F) than in the 40 W exposures (Figure 2 A−C). Although the coil temperature was not measured in this study, prior studies have shown that the coil temperature is higher at higher wattage settings.[38] As a result, higher coil temperatures volatilize more liquid into the gas phase, likely causing greater aerosol particle production once the airstream exits the mouth piece. Furthermore, at the 40 W exposures, the e-cig-generated aerosol of PG has more deposition than that of the GLY exposure (1.02 ± 0.136 versus 0.567 ± 0.0549 mg/cm^2, Figure 2A,B, respectively). We hypothesize that this is caused by the differences in chemical formulas and structures of PG and GLY. Both PG and GLY have C_3-backbones but with a difference of one hydroxyl group; specifically, GLY has one more hydroxyl group than PG, which means that the vapor pressure of GLY is lower than that of PG. Therefore, GLY lends itself to being more hydrophilic and forming more hydrogen bonds than PG, and this translates into the boiling point of GLY (290 °C)[31] being higher than that of PG (187.6 °C).[30] As a result, when heated by an e-cig, PG is more likely to aerosolize faster than GLY and therefore deposit more particles at the 40 W exposures.

For the studies described here, we focused solely on the humectants, PG and GLY, because, while there is a complex variety of e-cig products, nicotine formulations, and flavoring agents present on the market, all e-liquids contain some combination of PG and GLY. We exposed 16HBE cells to pure PG and pure GLY to determine the contribution of biological effects from each specific humectant, and there are e-liquids that are marketed as 100% PG and 100% VG or "Max VG". We also tested PG/GLY 55:45 v/v ratio, which is PG/GLY 50:50 mass/mass ratio, since this is a commonly used humectant mixture. PG and GLY are both rather innocuous and ubiquitous in cosmetics, pharmaceuticals, and food.[39,40] In our own research, nonaerosolized PG and the mixture of nonaerosolized PG/GLY at the same mass deposited in our 85 W aerosol exposures induced no changes in pro-inflammatory signals or cellular stress responses (Figure 8). The non-aerosolized GLY exposure did increase IL-6 gene expression (Figure 8A,B), but to a small degree. Similarly, in a subchronic rodent exposure model of inhaled nebulized (not heated) PG and GLY, no lung inflammation was observed and no changes in gene or protein expression were observed in the nasal epithelium of exposed rats.[41]

However, the whole aerosol mixture (gas and particle) of vaped PG and vaped GLY at both 40 and 85 W did increase IL-6 and IL-8 protein levels in the supernatants (Figures 4B,D,F,H). These results were similarly observed in another study that exposed airway epithelial cells (BEAS-2B) to vaped PG and GLY, which reported increases in IL-6 but not IL-8 levels.[35] Interestingly, another study exposing primary airway cells to PG and GLY did not show an increase in IL-6 or IL-8,[36] despite exposing cells to more e-cig generated puffs than those used in this study. The differences observed could be due several factors, including the use of different cell types/lines, differences in the exposure systems, electronic cigarette devices, and formulation of the e-liquid. Specifically, the e-cig device used in those studies are either first or second generation devices, whereas the study presented here uses a third generation device with a subohm coil, which allows for higher wattages to be achieved and more aerosol to be

generated. These differences could also explain the differences in cytotoxicity we have measured in comparison to previous studies.[35,42] We show here that PG vaped at high wattages can cause slight toxicity that has not been seen or measured previously. Interestingly, most of the biological effects measured in this study were with the e-cig generated aerosol of PG and GLY and not necessarily with the mixture of PG/GLY. (Figures 4 and 5). It is clear that while vaped PG and vaped GLY cause effects on their own, these effects are not additive when PG and GLY are vaped together.

Heating PG and GLY to the point of vaporization, as is the case in e-cigs, can produce harmful thermal degradation products such as aldehydes,[18] free radicals,[19,20] and reactive oxygen species,[43] which are mostly found in the gas phase of the e-cig aerosol.[44] Although we did not measure those compounds, it is very likely that the aerosols generated in the study presented here contains these compounds. To examine the contribution of gas-phase components in the effects we observed, we modified our exposure system by filtering out the particles from the aerosol of the vaped humectants with a HEPA filter. Our results indicate that the exposure of airway cells to the particle-depleted gas-phase components of the vaped humectants still increased pro-inflammatory and cellular stress responses, but to a lesser degree. One caveat of removing the particles is that we were potentially shifting the gas-to-particle partitioning equilibrium of any semivolatile organic compounds and thereby removing some portion of these compounds from the gas phase as well. Hence, the data shown in Figure 7 could present an underestimation of the gas-phase effects of the aerosol mixture. Ultimately, these data indicate the need for complete aerosol exposures with both the gas and particle in order to obtain a better understanding of the effects of e-cigs on airway epithelial cells. Previous studies that have used the pure compounds or conditioned media of collected aerosol particles in their exposures likely underestimate the full scope and magnitude of potential biological effects caused by aerosol mixtures. The main purpose of developing and optimizing the exposure system described here was to expose airway cells to the complete aerosol mixtures generated by e-cig devices, containing both the gas and particle phases. As mentioned above, many of the known toxicants of the vaped humectants are aldehydes, which can be found in the gas phase of the aerosol. However, the aerosol of vaped humectants can also contain formaldehyde hemiacetals, which are more likely to be found in the particle phase of the aerosol.[44,45] There has been a great deal of focus on determining what potentially harmful chemicals are in the gas phase of e-cig aerosol,[18−20,43] and very little focus on potentially harmful compounds in the particle phase of the aerosol.[45] We have determined that PG and GLY are the main chemical compounds in the particle phase of the aerosol but have also identified potential biomarkers of exposure (i.e., small oligomers) generated by the e-cig vaporization of PG and GLY, which have not been shown previously (Figure 3). It is possible that these oligomers may contribute to the toxicity we have measured, but future studies determining the chemical identification of these oligomers are necessary before we can begin to assess how and to what extent these oligomers contribute to the biological responses observed in this study. We chose to perform the chemical characterization with UPLC/ESI(+)-HR-QTOFMS out of concern that with higher operating temperatures of most gas chromatography (GC)/MS systems, any oligomers in the samples could thermally decompose (or fractionate).

In addition to pro-inflammatory end points, we analyzed the expression of NQO1 and HMOX1, which are both associated with cellular stress responses.[32,46] NQO1 and HMOX1 are both targets of the KEAP1−Nrf2 pathway, which is considered a master regulator of cellular responses to electrophilic and oxidative stress.[47] HMOX1 is the gene for the enzyme HO-1 which is the rate-limiting step of heme degradation, leading to the formation of bilirubin, CO, and ferritin, which all have antioxidant functions.[48] The protein product of NQO1 has versatile cytoprotective functions, including reducing quinones, quinoneimines, nitroaromatic compounds, and azo dyes to less reactive and damaging compounds, as well as functioning as a superoxide scavenger.[49] In cells exposed to the whole aerosol of vaped PG, GLY and PG/GLY at high wattages, there was an increase in NQO1 expression (Figure 5C), while only vaped GLY increased HMOX1 expression (Figure 5D) and its protein (Figure 5E,F). Additionally, vaped GLY at high wattages increased HMOX1 expression in hBECs. Differentiated hBECs are an exceptionally relevant *in vitro* model since they mimic morphological features of the human airways *in vivo* and contain at least three different cells types found in the airways, such as ciliated cells, secretory cells, and basal cells.[50,51] Hence, our data shown here provide support that these effects might occur in humans *in vivo*.

The increases in cellular stress-associated genes NQO1 and HMOX1 prompted us to investigate other markers of cellular stress, such as protein carbonylation, which is an irreversible oxidation of proteins and is used often as a marker of oxidative stress. Our data demonstrate that only the vaped GLY increases the levels of oxidized protein. Limitations of the carbonylation assay shown here include the inability to identify specific proteins oxidized by the aerosol exposure and or identifying the specific compounds causing the protein carbonylation. However, these data are particularly interesting because it has been reported that a higher ratio of GLY over PG in the e-liquid actually increases the formation of hydroxyl radicals when the humectants are vaporized by an e-cig device. Furthermore, the acrolein formed in the aerosol of the vaped humectants has been directly linked to the degradation of GLY.[18] Acrolein has been shown to activate the KEAP1/Nrf2 pathway,[33] induce the expression of NQO1 and HMOX1,[33,52] and adduct to proteins.[53] Hence, in addition to other e-cig variables, such as device settings, nicotine content, and flavorings, the ratio of PG/GLY could significantly affect the generation of harmful compounds and resulting biological effects.

Taken together, these data suggest that we have developed an *in vitro* e-cig exposure system that facilitates the exposure of relevant experimental models to the entire aerosol mixture, thus mimicking exposures of the respiratory mucosa after vaping e-cigs. Our results provide additional support to the emerging idea that vaporized humectants can cause adverse health effects on their own. A previous study using an *in vivo* 90 day exposure of rats to vaped PG and GLY showed increased levels of LDH and total protein, as well as numbers of macrophages and neutrophils in the bronchoalveolar lavage fluid (BALF), suggesting an inflammatory response.[54] In a more relevant human exposure setting, workers in the entertainment industry, who were frequently exposed to fog machines, which heat up a mixture of glycols to make the aerosol, had small but significant decreases in lung function as well as increased rates of coughing and wheezing.[55] Furthermore, there are different biological effects induced by

the gas- and particle-phase components of the vaped humectant aerosol mixtures, and more research is needed to determine what chemical byproducts could form from the vaporization of PG and GLY in the different phases of the aerosol, since that will determine deposition of these chemicals in the respiratory tract. These novel compounds could serve as biomarkers of exposure. This research emphasizes the need to regulate not only flavoring and nicotine in e-cigs but also the humectants PG and GLY since different ratios of these compounds can cause differential effects.

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Notes

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